Terasaki spiral ramps and intracellular diffusion

To cite this article before publication: Greg Huber et al 2019 Phys. Biol. in press https://doi.org/10.1088/1478-3975/ab4080

Manuscript version: Accepted Manuscript

Accepted Manuscript is "the version of the article accepted for publication including all changes made as a result of the peer review process, and which may also include the addition to the article by IOP Publishing of a header, an article ID, a cover sheet and/or an 'Accepted Manuscript' watermark, but excluding any other editing, typesetting or other changes made by IOP Publishing and/or its licensors"

This Accepted Manuscript is © 2019 IOP Publishing Ltd.

During the embargo period (the 12 month period from the publication of the Version of Record of this article), the Accepted Manuscript is fully protected by copyright and cannot be reused or reposted elsewhere.

As the Version of Record of this article is going to be / has been published on a subscription basis, this Accepted Manuscript is available for reuse under a CC BY-NC-ND 3.0 licence after the 12 month embargo period.

After the embargo period, everyone is permitted to use copy and redistribute this article for non-commercial purposes only, provided that they adhere to all the terms of the licence https://creativecommons.org/licenses/by-nc-nd/3.0

Although reasonable endeavours have been taken to obtain all necessary permissions from third parties to include their copyrighted content within this article, their full citation and copyright line may not be present in this Accepted Manuscript version. Before using any content from this article, please refer to the Version of Record on IOPscience once published for full citation and copyright details, as permissions will likely be required. All third party content is fully copyright protected, unless specifically stated otherwise in the figure caption in the Version of Record.

View the article online for updates and enhancements.
Terasaki Spiral Ramps and Intracellular Diffusion

Greg Huber$^1$ and Michael Wilkinson$^{1,2}$

1 Chan Zuckerberg Biohub, 499 Illinois Street, San Francisco, CA 94158, USA,
2 School of Mathematics and Statistics, The Open University, Walton Hall, Milton Keynes, MK7 6AA, England

E-mail: greg.huber@czbiohub.org, m.wilkinson@open.ac.uk
June 2019

Abstract. The sheet-like endoplasmic reticulum (ER) of eukaryotic cells has been found to be riddled with spiral dislocations, known as ‘Terasaki ramps’, in the vicinity of which the doubled bilayer membranes which make up ER sheets can be approximately modeled by helicoids. Here we analyze diffusion on a surface with locally helicoidal topological dislocations, and use the results to argue that the Terasaki ramps facilitate a highly efficient transport of water-soluble molecules within the lumen of the endoplasmic reticulum.
1. Introduction

The endoplasmic reticulum (ER) sheets consist of stacks of pairs of phospholipid bilayer membranes in the interior of eukaryotic cells [1]. The bilayers divide the cell into two distinct regions, illustrated in figure 1(a): the lumen of the ER enclosed between the doubled bilayers forms a single region which is connected throughout the cell, and which is also continuous with the nuclear envelope. The region complementary to the lumen is the cytoplasm (and also the nucleoplasm). As well as dividing the cell into two regions, the surfaces of the ER play an important role in organizing complex biochemical processes by acting as a substrate for membrane-bound protein complexes on both the luminal and cytoplasmic sides (e.g., ribosomes are attached to the cytoplasmic facing ER-sheet membranes). It is this role as a surface for catalysis that dictates the large surface area of the ER, but these extensive surfaces would create barriers to diffusion in both cytoplasmic and luminal compartments [2]. Specifically, a system of stacked bilayer membranes can act as a barrier to diffusion of water-soluble species in the directions perpendicular to the layers. This appears to present a challenge to the efficient operation of the cell.

It has been understood for some time that there are topological 'defects' in the layers of the ER. These are often represented as holes in the lipid bilayer system, with approximately catenoidal edge surfaces, as illustrated in figure 1(a), forming a set of 'windows' or fenestrae, as illustrated in figure 1(b). However, careful studies [3, 4] of the topological structure of the ER sheets have revealed that the layers have a type of screw dislocation, which have been named 'Terasaki spiral ramps' after their primary discoverer. These are illustrated schematically in figure 1(c). In this paper we argue that these spiral dislocations allow extremely efficient diffusive transport perpendicular to the plane of the membrane sheets.

![Figure 1. The interiors of eukaryotic cells are divided by the surfaces of the endoplasmic reticulum (ER). (a) Each of these surfaces contains a region termed the 'lumen', separated from the cytoplasmn by lipid bilayers. Edges of the ER may have a catenoidal cross-section. (b) The ER is sometimes pictured as being punctured by 'windows', allowing diffusion of water-soluble species throughout the cytoplasm. (c) However, careful analysis of serial-section transmission-electron micrographs reveals the presence of spiral dislocations termed Terasaki ramps.](image-url)
Small molecules are able to traverse the cell by diffusion, a consequence of the fact that the motion of each molecule is a random walk. For both fenestra and Terasaki ramps, a random-walk trajectory can allow a molecule to pass between regions of the cytoplasm separated by sheets of the ER. In the case of a window connecting layers of the ER (as illustrated in figure 1(b)), a molecule must diffuse to the aperture in order to pass between layers (as illustrated in figure 2(a)). In the case of a spiral dislocation, however, a path (such as that illustrated in figure 2(b)) which winds once around a spiral dislocation allows movement between two successive sheets of the endoplasmic reticulum, without having to make contact with the dislocation itself. Compared to the situation illustrated in figure 2(a), this represents a much weaker constraint on the subset of random walks which allow transport between sheets. Analogous and mathematically equivalent to the problem of diffusion in the cytoplasm adjacent to ER sheets is the complementary problem of diffusion within the ER lumen, since paths that wind around the dislocation will also connect the lumina of successive sheets. In fact, we will argue that, rather than being a structural curiosity, the Terasaki spirals solve both of these diffusion problems at once, and are an essential element in the efficient operation of eukaryotic cells.

The technical content of our paper is concerned with describing a model for diffusion in the endoplasmic reticulum, showing how the spiral dislocations allow efficient transport perpendicular to its layers. In section 2 we model the structure of the endoplasmic reticulum in the vicinity of a spiral dislocation as a helicoidal surface. We analyze the diffusion on a helicoidal surface, emphasizing the statistics of winding numbers of diffusive trajectories about its axis. In section 3 we show that, at large times, the statistics of winding numbers approach those of random walks in a plane, which avoid a disc centered on the position of the dislocation. We calculate the variance
of the winding number at large times. Having modeled a single dislocation, in section 4 we use our results to describe diffusion of a water-soluble molecule in the cell, modeling the endoplasmic reticulum as a set of sheets connected by spiral dislocations with an approximately helicoidal structure. Section 5 discusses the implications of our estimate. The dispersion is described by an effective diffusion coefficient which is proportional to the density of Terasaki ramps. We argue that the density of ramps that are present in the ER is sufficient to allow unimpeded diffusion of small molecules.

Our results are related to a previous treatment of diffusion in an extended lamellar medium with randomly scattered dislocations [5]. That earlier work used a different approach, which depends upon a regularization procedure, and yields an estimate for the perpendicular diffusion coefficient which is comparable to our own. We contrast the two approaches in our discussion (section 5). In [5] it was predicted that dispersion perpendicular to the plane of the lamellae is marginally superdiffusive (specifically, the variance increases faster than linear in time by a logarithmic factor). However, the prediction of superdiffusion was strongly criticized [6], and the issue was left unresolved. In section 5, and in an Appendix, we explain why this criticism is not relevant to our application.

2. Diffusion on a helicoid

The Teraski spiral ramps are screw dislocations connecting the layers of the endoplasmic reticulum. The axis of the spiral is a topological singularity, in the sense that if a path on the surface of the endoplasmic reticulum lipid bilayer makes a circuit about the axis, then the path ends up on another layer of the structure. The surface of the lipid bilayer structure is, however, smooth everywhere. A helicoid is a smooth surface which has the same topology as the Terasaki spiral. The Helfrich model [7] for the energy density of a biological membrane has a term proportional to the square of the mean curvature. Because the helicoid has zero mean curvature it is a plausible model for the shape of the Terasaki spirals; a more refined model is considered in [8]. We therefore begin our investigation of diffusion within the ER sheets by analyzing diffusion on a helicoidal surface.

A helicoid is a two-dimensional surface in three dimensions defined by the following parametric equations for the Cartesian coordinates \((x, y, z)\):

\[
\begin{align*}
    x &= r \cos \theta \\
    y &= r \sin \theta \\
    z &= \alpha \theta
\end{align*}
\] (1)

with \(r \geq 0\) (technically speaking, it is the half helicoid since the line \(r = 0\) represents an edge of the structure). We assume there is isotropic diffusion on the two-dimensional surface, with diffusion coefficient \(D\). There is a corresponding stochastic dynamics of the \(r, \theta\) variables. Because our particular interest is in the dynamics of the \(z\) coordinate, representing motion perpendicular to the sheets, we concentrate on analyzing the
dynamics of $\theta$ in the limit as time $t \to \infty$. For simplicity, in this section we consider diffusion in a cylinder of radius $R$, with the dislocation lying along the axis of the cylinder. Equivalently, we consider the motion to occur in the region $0 \leq r \leq R$, with $\theta$ unbounded. The length $R$ therefore represents a lateral size parallel to the plane of the sheets, which could be identified with larger cellular scales.

The problem of diffusion on a helicoidal surface is closely related to understanding the winding of a random walk about a point in the plane. Some classic works which address the distribution of winding numbers for diffusion on the plane are [9, 10, 11, 12, 13]. The plane-diffusion problem turns out, however, to be quite different, in that the winding number about a point has a long-tailed distribution with a diverging variance. This divergence arises because the direction of a diffusive trajectory changes discontinuously. Because an arbitrarily short path can wind around a given point, a typical trajectory can make an infinite number of windings around said point in any time interval, no matter how short. The calculations in [9, 10, 11, 12, 13] show that this is what actually happens. For our problem of helicoidal diffusion, however, the particle has to move a finite distance in the direction of the dislocation axis in order to wind around the dislocation. This implies that the winding-number variance on a helicoidal surface is finite.

We can introduce a local Cartesian frame describing points on the helicoid in the neighborhood of $(r, \theta)$, with coordinates $(X, Y)$. Because of rotational symmetry it is sufficient to take $\theta = 0$. The $X$ axis will be taken to lie in the radial direction, along a line of constant $z$, and the $Y$ axis is then tilted so that small increments $\delta y$, $\delta Y$ of $y$ and $Y$ are related by

$$\delta Y = \sqrt{r^2 + \alpha^2 r} \delta y.$$  \hfill (2)

Because a point makes diffusive motion on the helicoidal surface, we can assume that, in a small time $\delta t$, there is a corresponding diffusive motion on the tangent plane. The consequent small displacement on the tangent plane, $(\delta X, \delta Y)$, has a probability density function (PDF) which is the diffusion kernel for isotropic diffusion in two dimensions:

$$P(\delta X, \delta Y) = \frac{1}{4\pi D\delta t} \exp \left( -\frac{\delta X^2 + \delta Y^2}{4D\delta t} \right).$$  \hfill (3)

This implies corresponding random displacements of the parameters $\delta r$ and $\delta \theta$. If we can determine the first two moments of these displacements, we can write down a Fokker-Planck equation for the joint PDF $P(r, \theta, t)$ of $r$ and $\theta$:

$$\frac{\partial P}{\partial t} = \frac{\partial}{\partial r} \left[ -\frac{\langle \delta r \rangle}{\delta t} P + \frac{1}{2} \frac{\partial}{\partial r} \left( \frac{\langle \delta r^2 \rangle}{\delta t} P \right) \right]$$

$$+ \frac{\partial}{\partial \theta} \left[ -\frac{\langle \delta \theta \rangle}{\delta t} P + \frac{1}{2} \frac{\partial}{\partial \theta} \left( \frac{\langle \delta \theta^2 \rangle}{\delta t} P \right) \right].$$  \hfill (4)

The relations between $(X, Y)$ and $(r, \theta)$ are determined by first projecting onto the $(x, y)$ plane, then transforming to polar coordinates. We have $\delta x = \delta X$ and $\delta y = \delta Y$. The length $R$ therefore represents a lateral size parallel to the plane of the sheets, which could be identified with larger cellular scales.
\[ \delta Yr/\sqrt{r^2 + \alpha^2}. \] Then, noting that \( r^2 = x^2 + y^2 \) and using \( \sqrt{1 + a} = 1 + a/2 - a^2/8 + \mathcal{O}(a^3) \), retaining terms to second order in the stochastic fluctuations, we have

\[
\begin{align*}
\delta r &= \sqrt{(r + \delta x)^2 + \delta y^2} - r = \delta x + \frac{\delta y^2}{2r} + \ldots \\
\delta \theta &= \frac{\delta y}{r} - \frac{\delta x \delta y}{r^2} + \ldots.
\end{align*}
\]

Hence we find

\[
\begin{align*}
\delta r &= \delta X + \frac{r}{2(r^2 + \alpha^2)} \delta Y^2 + \ldots \\
\delta \theta &= \frac{\delta Y}{\sqrt{r^2 + \alpha^2}} - \frac{\delta X \delta Y}{r^2 + \alpha^2} + \ldots.
\end{align*}
\]

Noting that \( \langle \delta X^2 \rangle = \langle \delta Y^2 \rangle = 2D\delta t \) and \( \langle \delta Y \rangle = \langle \delta X \delta Y \rangle = 0 \), the statistics of the increments of the polar coordinates are, therefore,

\[
\begin{align*}
\langle \delta r \rangle &= \frac{rD\delta t}{r^2 + \alpha^2} \\
\langle \delta r^2 \rangle &= 2D\delta t \\
\langle \delta \theta \rangle &= 0 \\
\langle \delta \theta^2 \rangle &= \frac{2D\delta t}{r^2 + \alpha^2}.
\end{align*}
\]

The Fokker-Planck equation is therefore

\[
\frac{1}{D} \frac{\partial P}{\partial t} = \frac{\partial}{\partial r} \left[ \frac{\partial P}{\partial r} - \frac{r}{r^2 + \alpha^2} P \right] + \frac{1}{r^2 + \alpha^2} \frac{\partial^2 P}{\partial \theta^2}.
\]

Now consider the long-time behavior of the distribution of the angular variable, for the case where the motion is confined to a cylinder with radius \( R \) with the axis of the helicoid at its center. We assume that the radial distribution has reached equilibrium, and write

\[ P(r, \theta, t) = f(r)p(\theta, t) \]

where the radial component is the zero-flux steady-state solution of (8), satisfying \( f' = fr/(\alpha^2 + r^2) \) with solution

\[ f(r) = n_0 \sqrt{\alpha^2 + r^2} \]

where \( n_0 \) is a constant of integration. Noting that a uniform distribution on the disc of density \( n_0 \) corresponds to \( f(r) = n_0 r \), we see that \( n_0 \) can be identified with the density when \( r/\alpha \gg 1 \). We assume the distribution \( p(\theta, t) \) is normalized, so that its integral over \( \theta \) is equal to unity. If there is a single particle in a disc of radius \( R \), then

\[ 2\pi \int_0^R dr \ f(r) = 1, \]

so that when \( R/\alpha \gg 1 \), the density is \( n_0 \sim 1/\pi R^2 \).

Now consider the long-time behavior of \( \theta \). The statistics of the increments of \( \theta \) are specified in equations (7). Because the variance of \( \delta \theta \) depends upon \( r \), the long-time behavior of \( \langle \theta^2 \rangle \) is determined by averaging over the distribution of \( r \). The distribution
of $\theta$ has, in the long-time limit, a variance $\langle \Delta \theta^2 \rangle \equiv 2\bar{D}_\theta t$, with diffusion coefficient

$$\bar{D}_\theta = \frac{1}{2t} \int_0^t dt' \langle \delta \theta^2 \rangle_{t'}$$

$$= \frac{1}{t} \int_0^t dt' \frac{D}{r^2(t') + \alpha^2}$$

$$= D \int_0^R dr \frac{f(r)}{r^2 + \alpha^2}$$

(11)

where $R$ is the radius of the cylinder. The last step of (11) follows from replacing a time average with an ensemble average, and using the fact that $f(r)$ is the probability density function for $r$. Hence we find

$$\bar{D}_\theta = n_0 D \int_0^R dr \frac{1}{\sqrt{r^2 + \alpha^2}} = \frac{D}{\pi R^2} \ln \left[ \frac{R}{\alpha} + \sqrt{\left( \frac{R}{\alpha} \right)^2 + 1} \right].$$

(12)

In the case where $R/\alpha \gg 1$, this is

$$\bar{D}_\theta \sim \frac{D \ln(2R/\alpha)}{\pi R^2}.$$  

(13)

3. Winding number at a finite time

In section 2 we examined the diffusion of the rotation angle in a finite region, and used the idea that the diffusing particle approaches a uniform density at large times. In this section we consider how to evaluate the variance of the rotation angle in an unbounded region.

When $r \gg \alpha$, the Fokker-Planck equation (8) takes the same form as the two-dimensional diffusion equation. Because the diffusing particle has a low probability of being in the vicinity of the dislocation, this indicates that, for large time, the variance of the rotation angle will be determined by solving a conventional diffusion equation, with the center of the helicoid replaced by an impenetrable disc, with a radius $\epsilon$ which will be determined shortly.

Compare equation (13) with the case of diffusion in the plane around a disc of radius $\epsilon$. The corresponding angular diffusion coefficient is obtained by setting $\alpha = 0$, and introducing a lower cutoff of $\epsilon$ in the integration over $r$ in (11). This gives an equation which is identical to (13), except for replacing $\alpha/2$ with $\epsilon$, implying that a helicoid with pitch $\alpha$ has the same asymptotic winding number statistics as a planar diffusion around a disc of radius $\alpha/2$.

We have argued that the diffusion on a helicoid of pitch $\alpha$ is equivalent to motion on a flat surface with an excluded disc of radius $\epsilon = \alpha/2$ for trajectories which do not approach close to the axis of the helicoid. Now we use this observation to determine the distribution of winding angle $\Delta \theta$ when the starting point is at a distance $R$ from the axis, with $R/\alpha \gg 1$. 


The winding angle of a trajectory is

$$\Delta \theta = \int_0^t dt' \frac{\eta(t')}{r(t')}$$

(14)

where $r(t)$ is the distance of the diffusing trajectory from the center of the disc at time $t$, and $\eta(t)$ is a stochastic velocity of the diffusive trajectory in a direction perpendicular to its displacement from the dislocation. This satisfies

$$\langle \eta(t) \rangle = 0, \quad \langle \eta(t) \eta(t') \rangle = 2D \delta(t - t').$$

(15)

Using (15) in (14), the variance of the rotation angle is

$$\langle \Delta \theta^2 \rangle = 2D \int_0^t dt' \int_{\epsilon}^\infty dr \frac{P(r, R, t')}{r^2}.$$

(16)

where $P(r, R, t)$ is the probability density to reach a distance $r$ from the dislocation at time $t$, after starting at $R$ when $t = 0$. If there was no excluded disc, we would be able to obtain $P(r, R, t)$ exactly by integrating over the propagator for diffusion in two dimensions (equation (3)) over a circle, to obtain

$$P(r, R, t) = \frac{r}{4\pi D t} \int_{0}^{2\pi} d\phi \exp \left[ -\frac{(R - r \cos \phi)^2 + r^2 \sin^2 \phi}{4Dt} \right].$$

(17)

We are interested in the limit where the radius of the excluded disc is small compared to other length scales in the problem. As the radius $\epsilon$ of the excluded disc approaches zero, its effect on the density of diffusing trajectories becomes negligible, and we can approximate $P(r, R, t)$ using (17) outside the disc of radius $\epsilon$ (and it is obviously exactly zero inside). The variance of the rotation angle at time $t$ for a trajectory which starts at a distance $R$ from the dislocation is therefore

$$\langle \Delta \theta^2 \rangle = F \left( \frac{R^2}{4Dt}, \frac{\epsilon}{R} \right).$$

(18)

where

$$F(X, Y) = \frac{1}{2\pi} \int_{Y}^{\infty} \frac{dx}{x} \int_{0}^{1} \frac{dy}{y} \int_{0}^{2\pi} d\phi \exp \left[ -\frac{X}{y} (1 + x^2 - 2x \cos \phi) \right] \left( \frac{2Xx}{y} \right).$$

(19)

and $I_0(\cdot)$ is a modified Bessel function of the first kind and of order zero. This may be written in the form

$$F(X, Y) = \int_{Y}^{\infty} \frac{dx}{x} G(X, x)$$

(20)

where $G(X, x)$ is obtained by comparison with (19).

Let assume that $Y \ll 1$, and divide the integral over $x$ into two intervals: $[x_0, 1]$ and $[Y, x_0]$, with $Y < x_0 \ll 1$. If $G(X, 0) \neq 0$, in the limit as $Y \to 0$, the integral in (19) is dominated by the second of these contributions, and we may write

$$F(X, Y) \sim \ln(1/Y) G(X, 0) + g(X)$$

(21)
where \( g(X) \) can be expressed as a limit of a triple integral. The dominant term, logarithmic in \( Y \), is proportional to

\[
G(X, 0) = \int_0^1 \frac{dy}{y} \exp(-X/y) = \int_1^\infty \frac{dz}{z} \exp(-Xz)
\]

\[
= E_1(1/X) = -Ei(-1/X)
\]

where \( E_1(z) \) and \( Ei(z) \) are different standard specifications of the exponential integral function. We were not able to obtain the function \( g(X) \) which appears in (21) explicitly, but we were able to obtain a useful expression which is asymptotic to \( g(X) \) as \( X \to 0 \). The limit \( X \to 0 \) corresponds to the long-time limit, in which the distribution of diffusing trajectories becomes isotropic, so that we may drop the term in \( \cos \phi \) from the first line of (19), so that when \( X = R^2/4Dt \) is small

\[
\langle \Delta \theta^2 \rangle \sim \int_Y^\infty \frac{dx}{x} \int_1^\infty \frac{dz}{z} \exp[-Xz(1 + x^2)]
\]

\[
= \frac{1}{2} \int_1^\infty \frac{dz}{z} \exp(-Xz)E_1(XY^2z)
\]

\[
\sim \ln \left( \frac{1}{Y} \right) E_1(X) + \frac{(\ln X + \gamma)^2 - \pi^2/24}{4}
\]

where in the final line we use the fact that \( E_1(x) \sim -(\ln x + \gamma) \) when \( x \ll 1 \), together with equation 4.335.1 from [14] (\( \gamma \) is the Euler-Mascheroni constant). Note that this is in the form of equation (21). Recalling that \( \epsilon = \alpha/2 \), in the limit where \( R \gg \alpha \), the leading-order contribution to the variance of the winding number is therefore

\[
\langle \Delta \theta^2 \rangle \sim \ln \left( \frac{2R}{\alpha} \right) \int_1^\infty \frac{dz}{z} \exp \left[ -\frac{R^2}{4Dt} z \right].
\]

4. Model for perpendicular diffusion

We have analyzed diffusion on a helicoidal surface, leading to an estimate (24) for the winding angle of a trajectory after time \( t \), starting at a distance \( R \) from the dislocation. We now adapt the results to model diffusion perpendicular to the sheets of the endoplasmic reticulum, using the observation that its sheets are connected by multiple spiral dislocations. For definiteness, we consider diffusion within the lumen of the ER, but the basic arguments for modeling diffusion in the cytoplasm differ only in inessential points. This perpendicular diffusion process is described by keeping track of on which sheet of the lumen a molecule is located. Because the spiral dislocation singularities connect different sheets to form a single manifold, its subdivision into numbered sheets is somewhat arbitrary.

The layers of the endoplasmic reticulum, which we assume have mean separation \( h \), are connected by many of these dislocations, which will be assumed to be randomly scattered, with planar density \( \rho \). The dislocations may be either ascending or descending for a positive winding number, and we distinguish these cases by a ‘charge’ \( \sigma_i = \pm 1 \) for the dislocation with index \( i \). We shall assume that the distribution of these
Terasaki Spiral Ramps and Intracellular Diffusion

topological charges can be modeled by independently assigning each singularity a positive or negative charge, each with probability equal to one half. This net neutrality of topological charge is consistent with the census of Terasaki ramps from topological reconstruction of electron microscopy data [4].

If \((x, y)\) are the coordinates of the plane, we can describe the position by a single complex number, \(\zeta = x + iy\). If there is a dislocation at the origin, we can represent the height of the surface, \(z\) by writing \(z = h\theta/2\pi\), where \(h\) is the pitch of the screw axis, and \(\theta\) is the polar angle in the complex plane. If we write \(\zeta\) in polar coordinates, \(\zeta = r \exp(i\theta)\), we can model a single dislocation by means of the logarithm of a complex variable. This follows from noting that \(\ln(\zeta) = \ln r + i\theta\), so that \(z = (h/2\pi)\text{Im} \ln \zeta\) is a model for a dislocation at the origin. Similarly \(z = (h/2\pi)\text{Im} \ln (\zeta - \zeta_0)\) describes a dislocation at \((x_0, y_0)\), where \(\zeta_0 = x_0 + iy_0\). We can extend this to model the connected surface of the endoplasmic reticulum by considering the following function:

\[
z(x, y) = \frac{h}{2\pi} \text{Im} \ln \left[ \prod_i (\zeta - \zeta_i)^{\sigma_i} \right]
\]

with \(\zeta_i = x_i + iy_i\), where \((x_i, y_i)\) are points randomly scattered in some finite-sized region, with the charges \(\sigma_i\) being randomly assigned to \(\pm 1\) with probability \(\frac{1}{2}\). The spacing of the layers, \(h\), is assumed to be small compared to the typical distance between nearest-neighbor dislocations. In the context of modeling the ER, this model has the attractive feature that the height \(z\) is a harmonic function. This implies that, in regions where the gradient of \(z(x, y)\) is small, the surface approximates a minimal surface (that is, the mean curvature is everywhere zero).

The motion of a molecule is now described by a random walk in the \((x, y)\) plane, and its motion in the perpendicular coordinate \((z)\) is determined by the manner in which this path is threaded through the set of singularities. If we were dealing with closed paths, we could describe the vertical motion by determining the winding number of the path about each singularity, but the diffusive trajectory of a molecule is almost always described by an open path. We adopt the following convention: From each dislocation we take a line parallel to the \(x\)-axis, in the negative direction. We regard the transitions between layers as occurring when a path crosses one of these lines. A path with decreasing \(y\)-coordinate moves up a layer as it crosses a line attached to a positive dislocation, and down a layer if it crosses a line attached to a negative dislocation (see figure 3). In the case where the path is closed, this convention is equivalent to summing the winding numbers of the trajectory about each dislocation, weighted by their sign.

For a given path, we can define its winding number, \(n_i\), about a given dislocation with index \(i\), in terms of the number of times the line attached to the singularity is crossed counterclockwise, minus the number of clockwise crossings. The change in level of a given path is the sum of the winding numbers for each dislocation, weighted by the sign of the dislocation:

\[
\Delta z = h \sum_i \sigma_i n_i .
\]
Figure 3. Our model of the endoplasmic reticulum, summarized by equation (25), has dislocations with random sign $\sigma_i$ and random positions $r_i$. A Brownian trajectory can move between ‘levels’ of the multi-sheeted manifold. We define a convention for labelling the levels of the manifold by the considering when the trajectory crosses a set of lines.

Note that the spacing between levels is $h = 2\pi \alpha$ for the simple helicoidal model studied in section 2. When time $t$ is large, there will be many singularities which could have non-zero winding number, and the winding numbers will typically be large, so that we may approximate $n_i = \Delta \theta_i / 2\pi$, where $\Delta \theta_i$ is the winding angle of the trajectory about the singularity with index $i$.

Both the winding numbers $n_i$ and the signs of the dislocations $\sigma_i$ are random variables (with zero mean), so that $\Delta z$ is a random variable. The distribution of the vertical displacement, $\Delta z$, is conveniently described by its variance: for a fixed configuration of the signs $\sigma_i$, this is

$$\langle \Delta z^2 \rangle = h^2 \sum_i \sum_j \sigma_i \sigma_j \langle n_i n_j \rangle . \tag{27}$$

The correlation function of the winding numbers, $\langle n_i n_j \rangle$, can be computed, as discussed by Hannay [15]. However we shall perform a further average of (27) over the random signs $\sigma_i$. Because $\langle \sigma_i \sigma_j \rangle = \delta_{ij}$, the off-diagonal contributions to the double-sum are zero, so that the winding-number correlation function $\langle n_i n_j \rangle$ is not required for our calculation of $\langle \Delta z^2 \rangle$. When we average over the signs, the doubly-averaged second moment of $\Delta z$ is

$$\langle \langle \Delta z^2 \rangle \rangle = h^2 \sum_i \langle n_i^2 \rangle . \tag{28}$$

We have obtained the variance of the winding angle for a single helicoidal dislocation in equation (24). We now estimate the sum in (28) by replacing the sum by an integral.
over the density of dislocations at a distance \( R \) from a randomly chosen point. The expected number of dislocations in an annulus of width \( \delta R \) at distance \( R \) from the origin is

\[
\delta N = 2\pi R \rho \delta R
\]

where \( \rho \) is the density of dislocations. Using equations (28), (24), (29) and recalling that \( h = 2\pi \alpha \), we have

\[
\langle \langle \Delta z^2 \rangle \rangle = \frac{h^2}{2\pi} \sum_i \langle \Delta \theta_i^2 \rangle
\]

\[
= \frac{h^2 \rho}{4\pi^2} \int_0^\infty dR \ 2\pi R \langle \Delta \theta^2 \rangle_{R,t}
\]

\[
= \frac{h^2 \rho \Delta t}{2\pi} \int_0^\infty dX \ \ln \left( \frac{16\Delta t X}{\alpha^2} \right) \int_1^{\infty} \frac{dz}{z} \exp \left( -X z \right)
\]

\[
\sim \frac{h^2 \rho \Delta t}{2\pi} \ln \left( \frac{64\pi^2 \Delta t}{h^2} \right) \int_0^\infty dX \int_1^{\infty} \frac{dz}{z} \exp \left( -X z \right)
\]

\[
= \frac{h^2 \rho \Delta t}{2\pi} \ln \left( \frac{8\pi}{h} \right)^2 \Delta t \tag{30}
\]

where in the penultimate step we use the fact that \( \Delta t / h^2 \gg 1 \) for times large enough to allow non-zero winding numbers with a significant probability. This is the principal technical result of our paper. A similar, but not identical, result has been proposed for diffusion in an extended lamellar medium punctured by dislocations [5]. We comment on the relation between these results in the concluding section. Note that \( \langle \langle \Delta z^2 \rangle \rangle \) has a faster than linear growth, because of the logarithmic factor, implying that the dispersion in the \( z \) direction is marginally superdiffusive.

We can describe the dispersion across the layers of the ER by an effective diffusion coefficient, \( D_{\text{eff}} \). We define this by assuming that the size of the cell is \( \bar{R} \), and noting that the time \( \bar{t} \) for dispersion by conventional diffusion may be related to \( \bar{R} \) by writing \( \bar{R}^2 = 4\Delta t \bar{t} \). The effective diffusion constant for dispersion across the layers of the ER is defined by writing

\[
\langle \langle \Delta z^2 \rangle \rangle_{\bar{t}} = 2D_{\text{eff}} \bar{t} \tag{31}
\]

Using these definitions we find the effective diffusion coefficient perpendicular to the layers of the ER to be

\[
D_{\text{eff}} = \frac{D \rho h^2}{2\pi} \ln \left( \frac{4\pi \bar{R}}{h} \right) \tag{32}
\]

5. Discussion

We have argued that, relative to spiral dislocations, holes have a disadvantage when it comes to allowing perpendicular diffusive transport in the lumen and cytoplasmic space. This is because a dislocation allows perpendicular transport just by winding around the
singualr axis, whereas holes require that the trajectory has to go to the defect and pass through. This indicates that spirals allow very efficient perpendicular transport.

Our estimate for the effective trans-layer diffusion constant of our model, equation (32), differs from the bare diffusion coefficient \( D \) by a factor proportional to \( \rho h^2 \). Our model assumes that the singularities are distinct objects, which is equivalent to specifying that \( \rho h^2 \ll 1 \), in which case the perpendicular diffusion coefficient is smaller than the planar diffusion coefficient.

Values for the inter-sheet separation in the ER are typically \( h \approx 200\text{nm} \). The spacing of of dislocations is thought to be roughly \( 1\mu\text{m} \), hence we estimate that the small parameter is \( \rho h^2 \approx 4 \times 10^{-2} \). The characteristic size of the region occupied by the endoplasmic reticulum is comparable to the size of a cell, so \( \bar{R} \approx 20\mu\text{m} \). These estimates give

\[
\frac{D_{\text{eff}}}{D} \approx \frac{\rho h^2}{2\pi} \ln \left( \frac{4\pi \bar{R} h}{h} \right) \approx 5 \times 10^{-2}
\]

so that, while the perpendicular diffusion coefficient \( D_{\text{eff}} \) is smaller than the ambient coefficient \( D \), by a factor of approximately 20, it is still adequate to allow efficient transport of small molecules throughout the ER. While it is difficult to measure ER diffusivity in the three-dimensional cellular setting, particularly considering our present focus on diffusion in the direction normal to the ER sheets, a typical diffusivity for a small protein (say, GFP) in the ER has been found to be 20 - 30 times smaller than that of GFP in water (the latter being \( 10^{-10}\text{m}^2\text{s}^{-1} \)) [16]. Because of discrepancies in geometry and types of ER probed by existing experiments, the agreement is most likely spurious. However, the comparison demonstrates that the magnitude of the attenuation is comparable to what has been measured in these related contexts. We conclude that Terasaki ramps provide a means to overcome the barriers to diffusive transport faced by aqueous solutes in the eukaryotic cell. This naturally suggests the hypothesis that such topological ER structures are required for efficient diffusion in eukaryotes.

In a pioneering work, Gurarie and Lobkovsky [5] obtained estimates for the diffusion coefficient for a lamellar medium punctured by dislocations. In the case where the density of positive and negative charged dislocations is equal, their estimate for the dispersion perpendicular to the plane of the lamellae has a similar form to our equation (30), and it is pertinent to contrast the two calculations. The method used in [5] first performs an average over the disposition of dislocations for a given path, before averaging over the paths, whereas we perform the averages in the opposite order. If the steps could be performed accurately and yielding finite results, the order of averaging would be irrelevant. However, the approach of averaging over the position of dislocations is extremely difficult, if we hope to correctly account for the excluded disc surrounding every dislocation point. This is because, for a given path, many configurations of dislocations would have to be excluded. The approach used in [5] averages over paths and dislocation configurations as if they were independent: the paths are sampled from an ensemble of Brownian motions and the dislocation positions are a random scatter. This choice produces an infinite answer for the first average, because the variance of the
Terasaki Spiral Ramps and Intracellular Diffusion

The rotation number of a Brownian path about any given point is infinite. The calculation in [5] does indeed produce a result in the form of a divergent integral, which must be regularized. There is no apparent reason why this procedure should produce the same result as our calculation, but it too produces a result (using our notation) in the form \( \langle \Delta z^2 \rangle \sim (\rho h^2 Dt/8\pi) \ln(Dt/a^2) \) (their equation (11)). The diffusion coefficient in [5] differs from our own (which is the conventional choice) by a factor of 4 (see their equation (1)). Taking account of this difference, the coefficient in their equation (11) is in accord with our equation (30). However equation (8) of [5] appears to be in error, and equation (9) is difficult to verify because of ambiguities analogous to the Ito vs. Stratonovich dichotomy, so we are uncertain about the status of their result.

It is interesting to remark that, according to equation (30), \( \langle \langle \Delta z^2 \rangle \rangle \) increases faster than linearly as a function of time, despite the fact that the underlying mechanism is diffusion on a complex surface. If we were modeling diffusion in an extended medium, rather than a finite-sized cell, this would pose a problem, because the predicted dispersion would eventually exceed that of the underlying diffusion process, which is impossible. (This point was made in a comment on the work by Gurarie and Lobkovsky [5], which treated diffusion in an extended lamellar phase [6, 17].) While this issue is not directly relevant to our estimates of diffusion in a cell, it is instructive to understand the origin of the difficulty, and how it could be resolved if we were dealing with an extended system. We address this in an appendix.

While our results show that small molecules can access the entire cytoplasm by diffusion alone, this may only be part of the ER-transport story. There is recent evidence for active transport throughout the smooth ER involving fluid flow within ER tubules. This may be required for the transport of larger proteins through the ER lumen, and hence to the most distal locations in cells [18].

Acknowledgements. MW thanks the Chan Zuckerberg Biohub for its hospitality. The authors thank John Hannay for helpful discussions about [5].

6. Appendix

If we are only interested in diffusion within a the dimensions of a typical cell, then the logarithmic term in equation (30) does not indicate an error in the calculation. This is because \( t \) must become very large before the product of the small parameter \( \rho h^2 \) and the logarithmic factor exceeds unity, and diffusion would spread molecules uniformly across the cell before any superdiffusive behavior could be observed. If we were interested in diffusion in a homogeneous region however, it is necessary to consider how the formulation of the problem should be modified so that the logarithmic term does not eventually imply diffusion which is faster than that which would be observed without the membranes.

Our model for the height of the surface, equation (25), is not suitable for describing an infinite, homogeneous region. To make the model well defined we have to confine the singularities \( \xi_i \) to a finite region, for example a disc of radius \( R \). The fluctuations of the
product $\prod_i (\xi - \xi_i)^{\sigma_i}$ increase without bound as $R$ increases, indicating that equation (25) is not suitable to model an infinite region by taking $R \to \infty$. If we were interested in modeling an infinite region, we could replace (25) by

$$z(x, y) = \frac{h}{2\pi} \text{Im} \ln [f_R(r) + if_I(r)]$$

(34)

where $r = (x, y)$ and $f_R$ and $f_I$ are independent realizations of an ensemble of random functions. These functions can be assumed to have the following statistics:

$$\langle f(r) \rangle = 0, \quad \langle f(r)f(r + R) \rangle = C(|R|)$$

(35)

where $C(R)$ is the correlation function of the random fields. This model is, by construction, statistically homogeneous, and is therefore suitable as a model for an infinitely extended random surface. (However it does lack the property of being a harmonic function, which was desirable for modeling the ER.) The dislocations correspond to points where $f_R = f_I = 0$. The density of these points is readily determined by the Kac-Rice method [19, 20].

At first sight, it seems as if the calculation in section 4 would be directly applicable to this variant model (equations (34) and (35)). There is, however, a reason why the analysis does not carry over. In section 4, when we averaged over the distribution of signs $\sigma_i$, we assumed that they are completely random. It has been shown that the distribution of zeros of a statistically homogeneous random field must satisfy a ‘screening’ property, implying that the signs cannot be chosen at random [21]. For this reason, the calculation of section 4 cannot be applied to the case of an infinitely extended region.

References


Terasaki Spiral Ramps and Intracellular Diffusion


